

Boundary layer methods in Biomecanics

Simplified set of Navier Stokes Equations: Applications in Biomecanics

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Aim

- simplification of Navier Stokes equations
- thanks to asymptotic theory:

"Boundary Layer"

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Starting from Navier Stokes (Axi)

- we simplify NS to a Reduced set of equations
 - which contains the physical scales,
 - the most important phenomena
- much more simple set of equations: Integral equations (1D)
- $\bullet\,$ cross comparisons in some cases of NS/ RNSP/ Integral































reality?



straight pipe, smooth walls, symmetry



velocity profile



velocity profile



- simplified set
- deduced from orders of magnitude































final system





Rigid wall:
$$u = v = 0$$
















First given profile:



First given profile:

marching procedure

 \rightarrow

distribution of pressure is a result



or given pressure drop by Newton iteration on the entrance flux

Numerical resolution



finite differences, implicit in time









$$p^{given} \rightarrow u^*$$



$$\frac{u^* - u^n}{\Delta t} + NL(u^n) = -\frac{\partial p^{given}}{\partial x} + \frac{\partial}{r\partial r} \frac{\partial u^*}{\partial r}$$

$$p^{given} \to u^*$$
 $rv^*(R) = -\int_0^R r \frac{\partial u^*}{\partial x} dr$



$$\frac{u^* - u^n}{\Delta t} + NL(u^n) = -\frac{\partial p^{given}}{\partial x} + \frac{\partial}{r\partial r}r\frac{\partial u^*}{\partial r}$$
$$p^{given} \to u^* \qquad rv^*(R) = -\int_0^R r\frac{\partial u^*}{\partial x}dr \left| \frac{\partial R}{\partial t} \right|_{0?}$$



Newton on the pressure to obtain the boundary condition





Pressure is a result of the computation





- integral system (ID) is included in RNSP
- we compute a more real profile







$$Q = \int_0^R 2\pi r u dr$$



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$$\frac{\partial u}{\partial x} + \frac{\partial rv}{r\partial r} = 0$$



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$$\int_0^R 2\pi r dr \cdot \left(\frac{\partial u}{\partial x} + \frac{\partial r v}{r \partial r} \right) = 0$$



$$Q = \int_0^R 2\pi r u dr$$

$$\int_{0}^{R} 2\pi r dr \cdot \left(\frac{\partial u}{\partial x} + \frac{\partial r v}{r \partial r} \right) = 0 \longrightarrow \frac{\partial (2\pi R^2)}{\partial t} + \frac{\partial Q}{\partial x} = 0$$



 $Q = \int_0^R 2\pi r u dr$

 $\frac{\partial(2\pi R^2)}{\partial t} + \frac{\partial Q}{\partial x} = 0$



 $Q = \int_0^R 2\pi r u dr$

 $\tau = \frac{\partial u}{\partial r}$



 $Q = \int_{0}^{R} 2\pi r u dr \qquad Q_{2} = \int_{0}^{R} 2\pi r u^{2} dr \qquad \tau = \frac{\partial u}{\partial r}$



 $Q = \int_{0}^{R} 2\pi r u dr \qquad Q_{2} = \int_{0}^{R} 2\pi r u^{2} dr \qquad \tau = \frac{\partial u}{\partial r}$

$$\int \left(\begin{array}{c} \frac{\partial u}{\partial t} + u \frac{\partial}{\partial x} u + v \frac{\partial}{\partial r} u = -\frac{\partial p}{\rho \partial x} + v \frac{\partial}{r \partial r} r \frac{\partial u}{\partial r} \\ 0 = -\frac{\partial p}{\rho \partial r} \end{array} \right)$$



 $Q = \int_{0}^{R} 2\pi r u dr \qquad Q_{2} = \int_{0}^{R} 2\pi r u^{2} dr \qquad \tau = \frac{\partial u}{\partial r}$

 $\frac{\partial Q}{\partial t} + \frac{\partial Q_2}{\partial t} = -(2\pi R^2)\frac{\partial p}{\partial x} - \tau$



 $Q = \int_{0}^{R} 2\pi r u dr \qquad Q_{2} = \int_{0}^{R} 2\pi r u^{2} dr \qquad \tau = \frac{\partial u}{\partial r}$

 $\frac{\partial(2\pi R^2)}{\partial t} + \frac{\partial Q}{\partial x} = 0 \qquad \frac{\partial Q}{\partial t} + \frac{\partial Q_2}{\partial t} = -(2\pi R^2)\frac{\partial p}{\partial x} - \tau$



gives Q_2 as function of Q an τ as function Q



 $Q_2 = \int_0^R 2\pi r u^2 dr \qquad \tau = \frac{\partial u}{\partial r}$



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 $Q_2 = (\frac{4}{3}) \frac{Q^2}{\pi R^2}$ $\tau = (8\pi) \frac{Q}{\pi R^2}$



 $Q_2 = \int_0^R 2\pi r u^2 dr \qquad \tau = \frac{\partial u}{\partial r}$



 $Q_2 = \int_0^R 2\pi r u^2 dr \qquad \tau = \frac{\partial u}{\partial r}$

 $Q_2 = \frac{Q^2}{\pi R^2}$

 $\tau = F(Q)$



need of profile



"usual" ID equations are a simplification of RNSP

Choice of profiles









Choice of the family of simple profiles


In an unsteady flow it is natural to use Womersley

$$\frac{\partial u}{\partial t} + u\frac{\partial}{\partial x}u + v\frac{\partial}{\partial r}u = -\frac{\partial p}{\rho\partial x} + v\frac{\partial}{r\partial r}r\frac{\partial u}{\partial r}$$
$$0 = -\frac{\partial p}{\rho\partial r}$$



In an unsteady flow it is natural to use Womersley

Womersley profiles are solution of RNSP



In an unsteady flow it is natural to use Womersley



In an unsteady flow it is natural to use Womersley



gives Q_2 as function of Q an τ as function Q

Integral resolution



Numerical resolution: finite differences





IBL is included in RNSP















Viscous region: boundary layer



Viscous region: boundary layer

Integral resolution









steady/ or large convective acceleration



 $U_e S = cst$



steady/ or large convective acceleration













 U_e at the wall



U_e at the wall

is the velocity at the edge of the boundary layer $u(x,\infty)$ at "infinity"





$$\delta_1 = \int_0^\infty (1 - \frac{u}{U_e}) dn$$












Interactive Boundary Layer



Interactive Boundary Layer







Choice of the family of simple profiles

In a steady flow it is natural to use Falkner Skan

Interactive Boundary Layer



IBL is included in RNSP



RNSP includes usual ID equations RNSP includes Womersley profiles RNSP includes Boundary Layer Theories (IBL)



Comparisons



Comparisons

Integral/ ID



Comparisons





full Navier Stokes Castem/ FreeFEM



flow in arteries





introducing wall elasticity: $p(x,t) = k(R(x,t) - R_0)$

+ The boundary conditions: here hyperbolical ($R(x_{in},t)$ and $R(x_{out},t)$) given



week coupling

$$\frac{u^{n+1} - u^n}{\Delta t} + NL(u^n) = -\frac{\partial p^n}{\rho \partial x} + v \frac{\partial}{r \partial r} r \frac{\partial u^{n+1}}{\partial r}$$
$$v^{n+1}(R^n) = -\int_0^{R^n} \frac{r}{R^n} \frac{\partial u^{n+1}}{\partial x} dr$$



week coupling

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 $R^{n+1} = R^n + v^{n+1}(R^n)\Delta t$



week coupling

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$$v^{n+1}(R^n) = -\int_0^{R^n} \frac{r}{R^n} \frac{\partial u^{n+1}}{\partial x} dr$$

 $R^{n+1} = R^n + v^{n+1}(R^n)\Delta t \qquad p^{n+1} = k(R^{n+1} - R_0)$



Flow in an elastic artery: integral relations

- new integral equations: adapting Von Kármán integral methods

The key is to integrate the equations with respect to the variable $\eta = r/R$ from the centre of the pipe to the wall ($0 \le \eta \le 1$).

specific integral system improved compared to the classical ones



Figure 1: The displacement of the wall (h(x, t = 2.5)) as a function of x is plotted here at time t = 2.5. The dashed line (wom3(x,2.5)) is the Womersley solution (reference), the solid line (B.L.) is the result of the Boundary Layer code and the dots (intg) are the results of the integral method ($\alpha = 3$, $k_1 = 1$, $k_2 = 0$ and $\varepsilon_2 = 0.2$).



Constructed an inverse method







Example 2

Experiment O. Romain, J. Mazeyrat LISIF PVI

P. Leprince, M. Kerouia Hospital Pitié Salpétrière



Modelling

J. Frelat M. Destrade (LMM)



O. Romain, J. Mazeyrat LISIF PVI















- Flow in a stenozed vessel
- steady, rigid wall

Sylvie Lorthois (IMFT) Toulouse

RNSP Scales



Using:

$$x^* = xR_0Re, r^* = rR_0, u^* = U_0u, v^* = \frac{U_0}{Re}v,$$

 $p^* = p_0^* + \rho_0 U_0^2 p \text{ and } \tau^* = \frac{\rho U_0^2}{Re} \tau$

the following partial differential system is obtained from Navier Stokes as $Re \to \infty$:

RNSP: Reduced Navier Stokes/ Prandtl System





RNSP: Reduced Navier Stokes/ Prandtl System

$$\begin{aligned} \frac{\partial}{\partial x}u + \frac{\partial}{r\partial r}rv &= 0,\\ (u\frac{\partial}{\partial x}u + v\frac{\partial}{\partial r}u) &= -\frac{\partial p}{\partial x} + \frac{\partial}{r\partial r}(r\frac{\partial}{\partial r}u),\\ 0 &= -\frac{\partial p}{\partial r}. \end{aligned}$$



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+ The boundary conditions.


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- axial symmetry ($\partial_r u = 0$ and v = 0 at r = 0),

- no slip condition at the wall (u = v = 0 at r = 1 f(x)),
- the entry velocity profiles (u(0,r) and v(0,r)) are given

- *no* output condition in $x_{out} = \frac{x_{out}^*}{R_0 Re}$

- streamwise marching, even when flow separation.



RNSP: Reduced Navier Stokes/ Prandtl System

$$\frac{\partial}{\partial x}u + \frac{\partial}{r\partial r}rv = 0,$$

$$(u\frac{\partial}{\partial x}u + v\frac{\partial}{\partial r}u) = -\frac{\partial p}{\partial x} + \frac{\partial}{r\partial r}(r\frac{\partial}{\partial r}u),$$

$$0 = -\frac{\partial p}{\partial r}.$$

Parabolic Problem - Marching Problem

- axial symmetry ($\partial_r u = 0$ and v = 0 at r = 0),
- no slip condition at the wall (u = v = 0 at r = 1 f(x)),
- the entry velocity profiles (u(0,r) and v(0,r)) are given
- *no* output condition in $x_{out} = \frac{x_{out}^*}{R_0 Re}$
- streamwise marching, even when flow separation.





Testing asymmetry in the entry profile

The velocities in the middle for Comflo and RNS. Comflo uses here 50X50X100 points. Dimensionless scales!

Wall Shear Stress

Evolution of the WSS distribution along the convergent part of a 70% stenosis (Re = 500); solid line: Poiseuille entry profile; broken line: flat entry profile.

Boundary Layer/ Perfect Fluid

The boundary layer is generated near the wall δ_1 is the displacement thickness.

Boundary Layer/ Perfect Fluid

The displacement thickness acts as a "new" wall! →Interacting Boundary Layer (IBL)

IBL integral: 1D equation

$$\begin{aligned} \frac{d}{d\bar{x}}(\frac{\bar{\delta}_1}{H}) &= \bar{\delta}_1(1+\frac{2}{H})\frac{d\bar{u}_e}{d\bar{x}} + \frac{f_2H}{\bar{\delta}_1\bar{u}_e},\\ \bar{u}_e &= \frac{1}{(R^2 - 2(\lambda/Re)^{-1/2}\bar{\delta}_1)}. \end{aligned}$$

To solve this system, a closure relationship linking H and f_2 to the velocity and the displacement thickness is needed.

Defining $\Lambda_1 = ar{\delta}_1^2 rac{dar{u}_e}{dar{x}}$,

the system is closed from the resolution of the Falkner Skan system as follows:

if $\Lambda_1 < 0.6$ then $H = 2.5905 exp(-0.37098 \Lambda_1)$, else H = 2.074.

From H, f_2 is computed as $f_2 = 1.05(-H^{-1} + 4H^{-2})$.

IBL integral: 1D equation Simplified Shear Stress

A simple formula as been settled:

$$WSS = (\mu \frac{\partial u^*}{\partial y^*}) / ((\mu \frac{4U_0}{R})) \sim .22 \frac{((Re/\lambda)^{1/2} + 3)}{(1 - \alpha)^3}$$

IBL integral: Comparison with Navier Stokes (Siegel et al. 1994)

$$WSS = aRe^{1/2} + b$$

Coefficient a and b for the maximum WSS. solid lines with \triangle and "square" : coefficient a and bobtained using the IBL integral method ;

coefficient a derived from Siegel for λ = 3;
coefficient a derived from Siegel for λ = 6;
coefficient b derived from Siegel for λ = 3;
coefficient b derived from Siegel for λ = 6.

- Flow in a 2D stenozed vessel
- steady, rigid wall

Xavier Pelorson & Annemie van Hirtum (ICP Grenoble)

- Flow in a stenozed vessel
- steady, rigid wall

RNSP non dimensional

Fig. 2 A comparison between computed non-dimensional pressure for the three models (NS, IBL and RNSP, in this last case the wall has

Fig. 4 A comparison between computed skin friction divided by $(0.47 \times 2.07)(1-\alpha)^{-1}/\overline{\lambda}$, $\propto (1-\alpha)^{-2}Re^{1/2}$ for the three models.

(+) measured data, (\triangleright) Thwaites and (×) RNSP

Fig. 12 Normalised pressure position p_3 for $h_{min} = 1.45$ mm: (+) measured data, (\triangleright) Thwaites and (\times) RNSP

Fig. 14 Normalised pressure at position p_2 for $h_{min} = 3.00$ mm: (+) measured data, (\triangleright) Thwaites and (\times) RNSP

Fig. 15 Normalised pressure at position p_3 for $h_{min} = 3.00$ mm: (+) measured data, (\triangleright) Thwaites and (\times) RNSP

- Flow in a stenozed vessel
- steady, rigid wall
- non symetrical case

non symmetrical case

- RNSP
- modified integral method to take into account the transverse variation of pressure
- NS

PAROIS RIGIDES

non symmetrical case

- RNSP
- modified integral method to take into account the transverse variation of pressure
- NS

x

- Flow in a stenozed vessel/ aneurism
- unsteady, rigid wall

- Flow in a stenozed vessel/
- unsteady, rigid wall

- Flow in a stenozed vessel/ aneurism
- unsteady, rigid wall


















Up to now, the wall was rigid



we use a simple elastic model















- Flow in a collapsible tube
- unsteady, elastic wall, no inertia



Collapsible tube



 R^n gives p^{n+1}





х





0.06

0.1

0

0.02

0.04

0.08

0.12

0.1

0.14











Franz Chouly Yohan Payan (TIMC Grenoble)

Xavier Pelorson & Annemie van Hirtum (ICP Grenoble)

Obstructive Sleep Apnea Syndrome





RNSP + Ansys





(PreOp)



(PostOp)



Conclusion

- starting from Navier Stokes
 - set of simple equations RNSP
- set of more simple equations Integral

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- Good agreement with full Navier Stokes

Conclusion

- starting from Navier Stokes
 - set of simple equations RNSP
- set of more simple equations Integral
- Good agreement with full Navier Stokes
- "explain" the features of the flow
- boundary conditions for full NS
- real time simulation



OSA:





- Use <u>Acrobat Reader 7.05</u> to see animations
- Updated version may be <u>found here</u>.





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